



(19) Europäisches Patentamt
European Patent Office
Office européen des brevets



(11) Publication number:

0 650 738 A1

(12)

EUROPEAN PATENT APPLICATION

(21) Application number: 94116908.8

(51) Int. Cl.: **A61M 5/14, A61M 5/168**

(22) Date of filing: **26.10.94**

(30) Priority: **28.10.93 US 144460**

(71) Applicant: **MEDRAD, INC.**

(43) Date of publication of application:
03.05.95 Bulletin 95/18

Kappa Manor II,
271 Kappa Drive
Pittsburgh, PA. 15238-2870 (US)

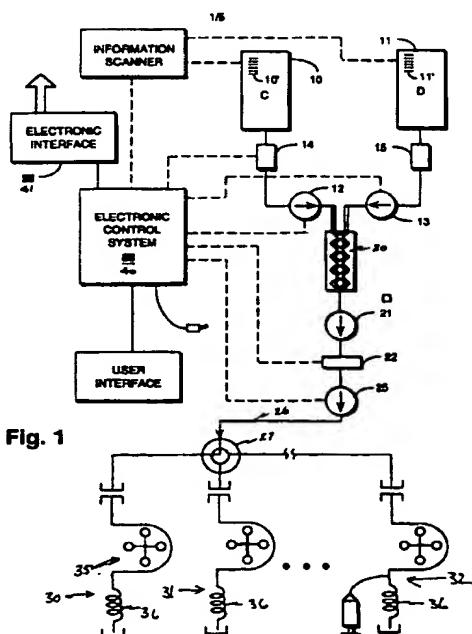
(84) Designated Contracting States:
DE FR GB NL

(72) Inventor: **Uber, Arthur E.III**
7426, Ben Hur Street
Pittsburgh
Pa.15208 (US)

(74) Representative: **Zinnecker, Armin, Dipl.-Ing. et al**
Lorenz-Seldler-Gossele,
Widenmayerstrasse 23
D-80538 München (DE)

(54) **Multi-patient fluid dispensing.**

(57) A system for delivering sterile fluid to a patient, while preventing cross-contamination, in which flow interrupting means are provided which basically create regions where no fluid exists in the comprehensive or over-all quality of material that is flowing from a fluid source to a patient.



EP 0 650 738 A1

BACKGROUND OF THE INVENTION

In copending application Serial No. 08/144,462 of even date herewith and assigned to the same Assignee as the present invention, discussion was undertaken with regard to the problems arising from the potential cross-contamination that can occur with a multi-patient fluid dispensing system. One facet of the system provided involves prevention of contamination of the multi-use segment of the fluid path during the time the system is connected to the patient. The disclosed system utilized one of two methods: a back flow preventing valve and a sterile filter, or a physical separation achieved by filling a dose container and separating the dose container from the filling fluid path before connection to the patient.

A back flow valve and a sterile filter combination should give sufficient protection. Bacteria cannot penetrate the filter. Viruses and proteins can penetrate the filter but are not active, and so cannot swim upstream. They can only diffuse. The drawbacks to this approach involve the pressure drop through the filter and volume of fluid remaining in the filter. Also, there is no way to verify that the filter is not leaking.

The present invention deals with additional methods of preventing contamination of the reusable fluid path by the patient being injected. To achieve the improved methods of preventing contamination, the present invention embodies the concept of preventing back flow, by providing no open fluid path through which bacteria can migrate or viruses or pyrogens can diffuse. (If a path is open, the velocity can then be made sufficient to prevent back diffusion.) Additionally, turbulence must be avoided since turbulence necessarily involves reverse flows and eddys that can carry material against the flow, unless the flow is high enough to prevent any part of the fluid from having a net upstream velocity vector.

Means of preventing contamination of the fluid path by contaminants other than the patient being injected are presented in copending application 08/144,462. Any of the concepts presented there may be matched with any of the embodiments presented here. The relevant feature is the "per patient" connection.

OBJECTS OF THE INVENTION

It is a principal object of this invention to provide an improved apparatus for injecting a fluid medium into a plurality of patients while minimizing the chance of cross-contamination.

It is another object of this invention to provide an apparatus for injecting fluid mediums into patients in which there is no continuous stream of

fluid existing between the source of the fluid and the patient.

It is another object of this invention to provide an apparatus in which a peristaltic apparatus is present which precludes the reverse flow of substances from the patient towards the origin of the fluid to be injected.

Other objects and advantages of this invention will be in part obvious and in part explained by reference to the accompanying specification and drawings in which:

DESCRIPTION OF THE DRAWINGS

- 15 FIG. 1 diagrammatically shows an apparatus and a system for injecting a fluid medium directly into a patient which minimizes the chance of patient-to-patient cross-contamination;
- 20 FIG. 2 is a form of peristaltic control apparatus that can be used in the cross-contamination preventing system of FIG. 1;
- 25 FIG. 3 is a front perspective of the apparatus of FIG. 2;
- 30 FIG. 4 is another diagram showing another type of peristaltic apparatus for use in the present invention;
- 35 FIGs. 5a and 5b are diagrammatic illustrations of an apparatus in which there is a biased element to preclude reverse flow of fluid from the patient towards the source of medical fluid;
- 40 FIG. 6 is a diagrammatic view showing one form of an apparatus for creating a discontinuous flow of medical fluid;
- 45 FIG. 7 is a diagrammatic showing of another type of apparatus having discontinuous flow and a plurality of patient connections;
- 50 FIG. 8 is a diagrammatic showing of a packeted flow means;
- 55 FIG. 9 is a diagrammatic showing of a disposable burette system; and
- FIG. 10 is a diagrammatic showing another system for packeting flow means.

DESCRIPTION OF THE INVENTION

- 45 To better understand the present invention, reference is made to the drawings, and specifically to FIG. 1 there is provided a source of fluid medium which is contained within a bulk container 10. Numerical 11 represents a similar container that is used to hold a supply of diluent, in the event that it is desired to reduce the concentration of the fluid medium contained within source 10. A metering pump 12 draws fluid from the supply source 10 at the proper flow rate. The second metering pump 13 draws diluent (when desired) from the bulk reservoir 11 within which the supply of diluent is contained. A preferred metering pump is a precip-

sion peristaltic pump with santoprene tubing. A pump wall design similar to that of U.S. Patent No. 5,236,014 would minimize the pulsatile flow characteristics. As the fluids are removed from containers 10 and 11, they are heated by means of heaters 14 and 15 so that they approximate body temperature. The heating, of course, can decrease the viscosity and make the fluid more comfortable for the patient. Upon leaving the metering pumps 12 and 13, the fluids meet as they are joined and flow through a static mixer 20 that contains helical vanes. The company ConProTech makes many sizes and lengths, some with polypropylene vanes and case. These static mixers are designed for mixing fluids with very different viscosities and varying dilution ratios. The exact length and diameter to be used will depend to some degree upon the viscosity of the substances being co-mingled. The mixture then flows through a fluid assurance device 22 which may be an ultrasonic detector so that the presence or absence of air in the fluid can be determined. Since these types of devices cannot detect small air bubbles, by being located before a pressurization pump 25, bubbles will be as large as possible. It helps minimize the chance that a broken line or human error can inject air into the patient. From pressurizing pump 25, a supply conduit 26 leads to a rotary switch 27 that can distribute fluid between the individual or "per patient" hookups 30, 31 and 32. Each of the individual connections contains what has been diagrammatically shown as a section to mate with a peristaltic apparatus 35. Each per patient disposable tube 36 is placed in a peristaltic apparatus 35 before being connected to the patient. Then it is connected to the patient and the injection is completed. The disposable connector tube 36 is disconnected from the patient. The rotary valve is turned to seal off the opening and the tube removed from the peristaltic apparatus and the connection to the rotary valve. This portion is then discarded. The next tube should be placed in the peristaltic apparatus.

This is a good strategy but it requires operator vigilance to make sure that the line is in the peristaltic device before being connected to the patient and that the rotary valve is moved before the line is removed from the peristaltic device. Interlocks and intermediate all/off positions on the rotary switch could be provided. The rotary valve could have a "no connection" position between each connection position. The interlocks could function such that the rotary valve cannot be moved to access an output line until the line is in the peristaltic device, and another interlock could require that the rotary valve be turned to the intermediate off before the tubing can be removed from the peristaltic pump.

The present apparatus includes an electronic control system (ECS) 40 to assure that the needs of the patient are met safely. ECS 40 gets information on the contents of the bulk reservoirs 10 and 11. The preferred method is to read bar codes indicated by numerals 10' and 11' respectively. Another way is to quiz the operator to enter the data each time a bulk reservoir is changed, and then store that information. The operator would read the label on or packaged with the bulk reservoir, and enter the appropriate data. This need only be done when a bulk reservoir is changed.

With each injection, the operator needs to tell the system what to do. The data most similar to present practice is: 1) the concentration desired, 2) the flow rate, and 3) the total volume to be delivered. Present practice also includes multiple phases with various flow rates during each phase. This system would allow various contrast concentrations during each flow rate as well.

However, given the capabilities of this system, a preferred set of information is: 1) the procedure being done, and 2) the patient weight. This way the contrast dose could be optimized for the patient. The algorithm would have been previously provided information on milligrams of iodine per kilogram of patient for each procedure when the system was first installed in the hospital. It could display concentration, flow rate and volume for operator verification, if the operator desired. An electronic interface 41 is shown which can connect to the hospital information system to get information on the patient, such as weight. Then the operator would only have to input the patient number. The electronic interface could also be connected to the imaging equipment. It could send or receive information so that, for instance, the operator only need to program the CT scanner with number of slices and body section, and this would be transmitted to the contrast delivery system to be used in determining flow rates and delays. The electronic interface would also be used to let the scanner trigger the contrast delivery system or vice versa, after the appropriate delays. A hard copy printer may be optionally part of the user interface, receiving data from the ECS. This can print a record of the actual injection for insertion into the patient records. The output may be alphanumeric or be a graphical representation of the injection.

The operation of delivering fluid to the patient can be started by the operator with a start switch on the contrast delivery system, or from the console of the scanner. There would need to be an arming procedure similar to that of present injectors to help assure patient safety.

In CT, usually only one injection is given, sometimes with pauses and changes in flow rates. As the end of the injection is reached, contrast can

be conserved if the contrast flow is stopped and the diluent flow continued so the "bolus" of diluted contrast is flushed out of the tubing and into the patient. In angiography, several injections may be used. It is necessary to flush only after the last injection, although no harm, except injecting a little extra fluid, occurs if the flush follows each injection.

Another form of waste is using contrast to prime the fluid path which is disposed of with each patient, especially if the concentration has not yet been decided upon. The flush or diluent fluid is much cheaper than the contrast and of lower viscosity, so it can be used to prime the line and make sure that all air has been removed from the path to the patient.

Referring to FIGS. 2 and 3 an alternative would be to make the peristaltic mechanism be fixed with the tubing, rather than separate as shown in FIG. 1. It would be disposable, but, it could be a very simple disposable with four wheels on a cross and a band which held the tubing for one or more turns. (It could be less than one turn, but one or more is preferred to equalize the lateral forces.) This type of construction is shown in FIGS. 4 and 3 with numeral 50 indicating the wheels mounted on cross 51 and in contact with supply tubing 52. FIG. 4 shows an even simpler arrangement where the wheels form a planetary gear set 60, with the inner gear free to rotate. In this embodiment, it might be easier to have the ratchet mechanism on the band as shown at 61 in FIG. 3. This whole assembly does not need to be more than 1" across. While the peristaltic pump never has an open fluid path, turbulence can move material from the wall to the wall farther upstream. Thus, it is desirable, but not essential, that the tubing diameter be chosen to preserve laminar flow. Since the flow ranges differ by modality, the Reynolds number calculation, familiar to fluid mechanics, will need to be used to make this determination.

The peristaltic mechanism could be used as a flow sensor. It could be coupled to a shaft on the durable equipment or an optical sensor could detect when the gears pass. Another use of the peristaltic flow sensor is as a mechanical stop. Peristaltic flow sensor could be placed on the durable equipment in such a way that the ECS 40 read the number of revolutions and stop its rotation when the appropriate volume was reached. Because the peristaltic flow sensor has some friction, it also prevents flow through caused by gravity when the system is off. The integral disposable peristaltic mechanism would limit dripping when the "per patient" disposable is removed. This "per patient" disposable peristaltic pump would also be a convenient pumping means for other low pressure IV fluid injections.

In all the peristaltic mechanisms above, any type of peristaltic motion is acceptable. A linear peristaltic mechanism would work. Two lines may be run in parallel through out of phase peristaltic mechanisms and their outputs combined to significantly decrease pulsations.

Also, it is important to note that a peristaltic mechanism while effective is not sufficient to prevent cross-contamination, if turned backwards, either by operator action or by back pressure, for example. There should be back flow prevention means in the line, or preferably in the peristaltic mechanism itself.

FIG. 8 shows another means of dividing the fluid flow into discrete packets to prevent cross-contamination. This is a variation on the peristaltic idea, where the fluid path splits into two parts. In this picture, fluid is flowing into chamber 1, its outlet is blocked so the chamber expands and drives the pressure plate against chamber 2. This drives fluid out of chamber 2 and on to the patient. When the pressure plate reaches the maximum designed travel, the inlet and outlet valves switch position, allowing chamber 2 to fill and chamber 1 to empty. This allows continuous fluid flow but never permits a continuously open fluid path to exist. It is preferred that the pressure plate upon reaching its end of travel mechanically trigger the inlet valves, and that there be a mechanical linkage between the valves so that they can not both simultaneously open to the same chamber. These controlling strategies could also be performed by the ECS, with redundancy and verification of valve positions. It is possible to extend this concept to using three or more chambers, to get a more even flow.

FIG. 10 shows another implementation of packetizing of the fluid flow. In this embodiment it is accomplished via air separation rather than via an intervening solid. After the fluids are mixed, they flow through a back flow valve. The fluid then flows through a "y" where it is mixed with packets of air. The air packets separate fluid packets, preventing back diffusion or migration of contaminants if the flow slows or stops. The wall material and diameter of the tubing is chosen so that the air packets are stable. During operation, fluid and air flow down the line to the air separating chamber. Here air separates itself from the fluid and moves upward through a filter, returning to be used again. Fluid flows on to the pressurizing pump. The pulsatile air pump could be a peristaltic pump, possibly operating out of phase with the fluid metering pumps so that air is injected when liquid flow is minimum from the metering pumps. After the air is separated from the liquid, the liquid flows through a fluid assurance device, is pressurized by the pressurizing pump and flows into the patient. The ECS will

stop the pumping if the fluid assurance detector detects any air in the line to the pressurizing pump. All of the tubing down stream from the "per patient" connector is disposed of after each patient. If the flow from the metering pumps is sufficiently pulsatile, it may not be necessary to have the air pump. The momentum of flowing fluid can be sufficient to entrain packets of air between packets of fluid.

In another embodiment, see specifically FIGS. 5a and 5b, there is provided a spring loaded conical section 65 which is contained in a conical housing 66. Since this arrangement has an open fluid path when fluid is flowing, it is desirable to maintain laminar flow. This configuration has the advantage that the width of the flow path increases to accommodate increased flow. The frontal area at cross section (A), the slope of the cylinder walls and the strength of the spring can be chosen to assure that the Reynolds number stays in the laminar flow region over the designed operating range. The pressure drop and speed of flow need to be high enough that no material can diffuse against the flow. The conical surfaces need to be chosen so that they mate over a wide length. A single line of sealing is not desirable. Multiple lines of sealing are better but not the best.

It may be that redundancy is achieved by having several conical blockers in series, or conical blocker in series with a peristaltic blocker. These could be combined with sterile filters or with air gaps as set forth below. While any one can be sufficient alone, the combinations may be needed to satisfy the perceptions of the patients or hospital personnel.

Referring to FIGS. 6 and 7 of the drawings, these embodiments use similar principals but they have an air gap as the blocking means to preclude cross-contamination. Bacteria and viruses which are in a fluid cannot become airborne unless the fluid is dispersed into the air.

Present hospital practice uses drip chambers, in which fluid drips through air. They are used with most IV injections. These drip chambers are designed for flow measuring. They are part of single use disposable devices and so have no relation to cross-contamination prevention.

Present art also included disposable burettes (FIG. 9) which can be filled from a sterile container and fluid in them then subsequently steriley dispensed. If filled once and then dispensed into a patient, the bulk source is protected from back flow of contaminants from the patient. But if any attempt is made to have fluid flow into the burette while connected to the patient and the bulk source, they do not provide a cross-contamination barrier. This is because fluid flowing into the burette falls some distance and can cause a splash which has a

possibility of carrying fluid from the bottom of the burette to the inlet nozzle. When fluid is being let out, low flow rates allow back migration of bacteria or back diffusion of virus or pyrogens. Subsequent splashing can bring these contaminants to the inlet and contaminate the remainder of the fluid path. Thus, in the embodiments below, great care is taken to eliminate potential splashing which can carry fluid across the air gap.

FIG. 6 shows a closed, sealed funnel 70 into which the fluid is tangentially injected near the top. The fluid flows around and down to the exit 71. The funnel is made of a hydrophobic plastic or has a hydrophobic coating so no string of fluid remains after flow is stopped. The area of the inflow tube and the flow rate are the variables which control the velocity of the fluid when it enters the funnel. These are chosen so a single stream, with a decreasing velocity as it flows toward the outlet, adheres to the wall of the funnel under the various flow rates for the specific application. This will eliminate splashing when the fluid stream meets the fluid pool in the bottom of the funnel. Fluid assurance devices 22 and pressurizing pump 25, etc., similar to equipment shown in FIG. 2, are found downstream from funnel 70.

In operation, the fluid injector is armed. When the start button is depressed, the metering pumps (not shown) start immediately. Mixed fluid flows into the top of the cone and collects at the bottom. This continues until several milliliters has collected in the cone and funnel geometry. The exact amount depends upon the programmed flow rate. The size of the cone needs to be sufficient to contain at least one second's worth of fluid at the programmed flow rate. After pre-filling the cone, the pressurizing pump is started. It pulls fluid from the cone and injects it into the patient. For low pressure applications, the pressurizing pump could be a peristaltic pump. For higher pressures, it preferably is a gear pump, although other types would do. Because the fluid contacting part is disposable, the gear head would be plastic, probably polycarbonate, and would mate to the durable equipment and be turned by it.

If there is air in the funnel, then there needs to be a fluid assurance device 22 at the outlet tube of the funnel, so that if something fails and the funnel is not filled, the ECS to can stop the pressurizing pump 25, preventing air from being pulled from the funnel and being delivered to the patient. There could also be a second fluid assurance after the pressurizing pump for redundancy. This would be especially useful for intra-arterial injections where air injection has much more serious consequence than during IV injections.

A second embodiment for the class of blocking means farming a break in the fluid stream uses a

collapsible bag 75, as shown in FIG. 7, or other large container instead of the funnel. Operation is a little different. When the arm sequence is initiated, a significant fraction of the fluid requested for the injection is pumped into the collapsible bag. This fraction could be operator controlled and depend upon the confidence the operator had that the full amount of fluid will be used. When the operator depresses the start switch, the injection starts. The metering pumps continue filling the bag at a slower rate than the pressurizing pump is withdrawing it, with the fill rate chosen so that filling is completed a few seconds before the injection is completed. The benefit of this over the funnel is the ability to start the injection and change flow rates instantaneously. The bag may be less costly than the funnel although neither part sees high pressures. A final benefit may be user perception. They may have more confidence in a device which fills an intermediate bag than in a system where there are just a few milliliters of fluid in a funnel, even though electronics and mechanics make them equally reliable.

As with the funnel, the bag needs to be made from hydrophobic material such as polypropylene so that no continuous stream of fluid remains after flow is stopped. The flow entering the bag needs to be slowed by choice of inlet diameter and tangential path so that it adheres to the wall and no splashing occurs.

While not ideal, it is possible to eliminate the static mixer by filling the bag, providing ultrasonic agitation and then pumping the mixture out. This is not as desirable because concentration cannot be changed during delivery.

By properly sizing the funnel or the bag, the need for a back flow preventer is eliminated. If the total volume of the fluid path down stream from the funnel or bag is less than the volume required to fill the funnel or bag, then back flow can never breach the air gap. If the funnel or bag volume is less than the down stream fluid path volume, then a back flow valve is needed.

It is also important that the funnel or bag be held in the proper upright position during use, since gravity is being used to assure that air surround the inlet port.

Claims

1. In a system for delivering sterile fluid to a patient, the combination comprising:
 - (a) a source of sterile fluid;
 - (b) a fluid delivery system for directing the sterile fluid from the source to a point of use in conjunction with a patient, and
 - (c) flow interrupting means in said fluid delivery system for causing the flow of the

fluid to be discontinuous so that fluid free gaps exist in the delivery system to preclude cross-contamination.

- 5 2. A system as defined in claim 1 wherein said flow interrupting means comprises physical means that cause the flow to exist as discrete quantities.
- 10 3. A system as defined in claim 2 wherein a portion of said fluid delivery system including that portion in contact with the patient is disposable and the remainder of the system is reusable.
- 15 4. A system as defined in claim 1 wherein said flow interrupting means comprises a peristaltic flow mechanism.
- 20 5. In a system for delivering sterile fluid to a patient, the combination comprising:
 - (a) a source of sterile fluid;
 - (b) a fluid delivery system for directing the sterile fluid from the source to a point of use in conjunction with a patient, and
 - (c) flow interrupting means comprising a hydrophobic surface over which the fluid is caused to flow.
- 25 6. A system as defined in claim 5 wherein said flow interrupting means comprises a receptacle having a generally funnel-shaped configuration.
- 30 7. A system as defined in claim 6 wherein said receptacle is sealed and has an inlet opening located to cause fluid flow to impinge the internal surface of said receptacle tangentially.
- 35 8. A system as defined in claim 1 wherein said fluid delivery system includes means for directing fluid to multiple patients and wherein each fluid directing means includes flow interrupting means.
- 40 9. A system as defined in claim 8 wherein valve means is provided to selectively operate each of said fluid directing means.
- 45 10. In a system for delivering sterile fluid to a patient, the combination comprising:
 - (a) a source of sterile fluid;
 - (b) a fluid delivery system for directing the sterile fluid from the source to a point of use in conjunction with a patient, and
 - (c) a valve having fluid flow control means that is positively biased towards a flow interrupting position.

11. A system as defined in claim 10 wherein said biased fluid flow control means is shaped to create laminar fluid flow where passing fluid.

12. In a system for providing a plurality of individual outlets for the sequential delivery of sterile fluid free of cross-contamination, the combination comprising:

- (a) a source of sterile fluid;
- (b) a sterile fluid conducting network connected to said source of sterile fluid, said conducting network including a fluid supply manifold and a plurality of individual outlet means connected thereto; and
- (c) flow control means disposed within said fluid conducting network effective to cause flow of the fluid in said conducting network to exist as discrete quantities.

13. A system as defined in claim 1, wherein said flow interrupting means comprises means for dividing the fluid flow by alternately opening and closing inlet and outlet valves.

5

10

15

20

25

30

35

40

45

50

55

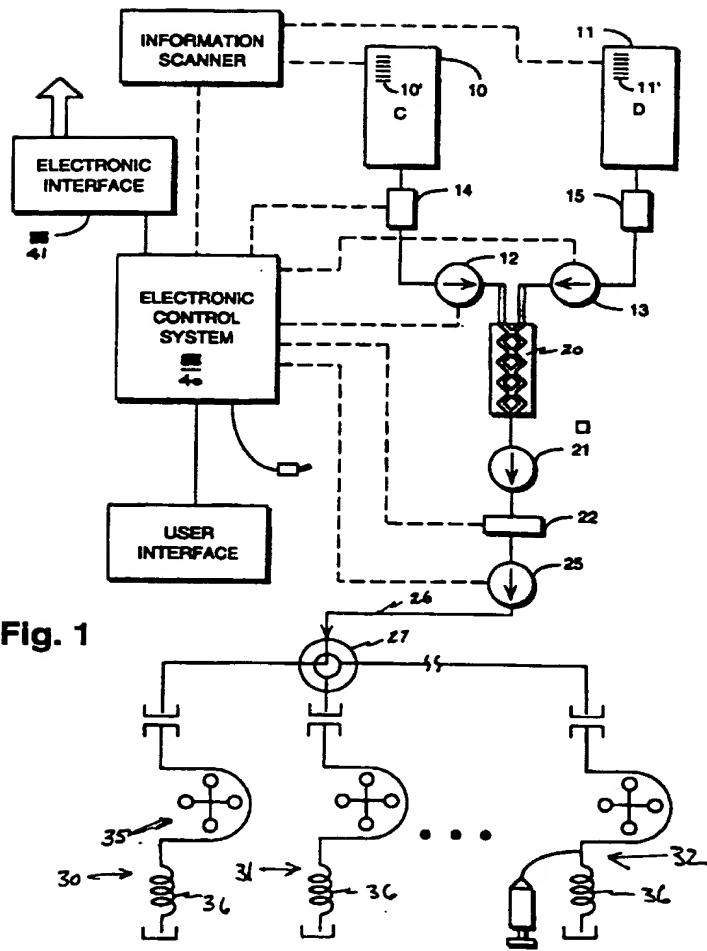
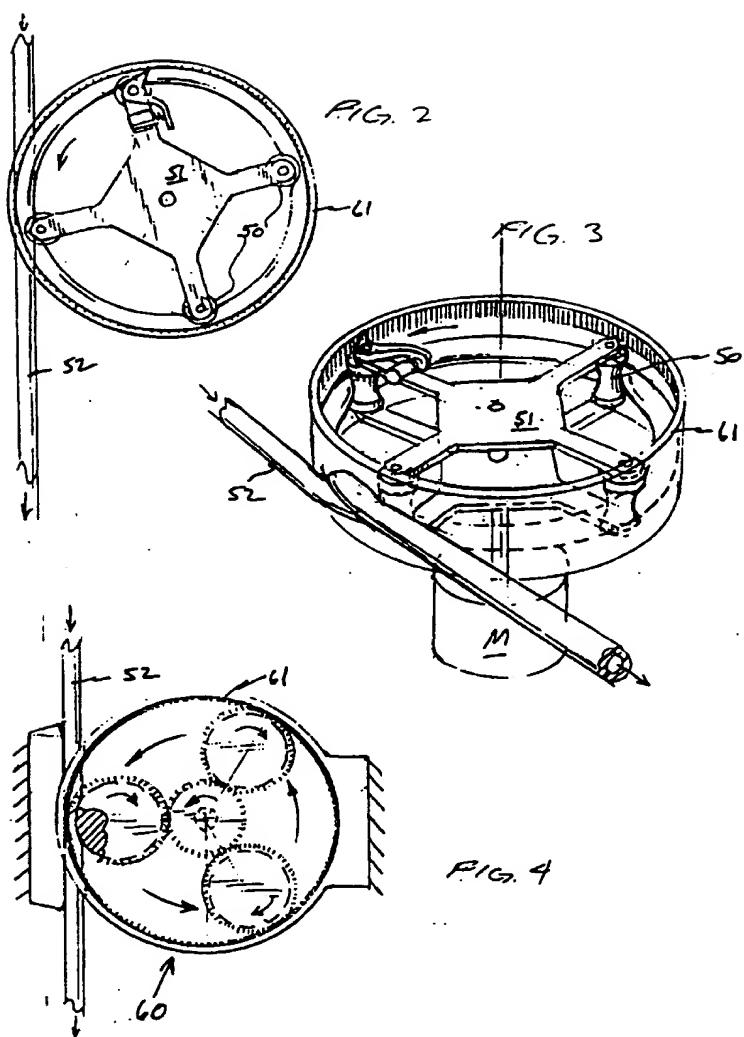
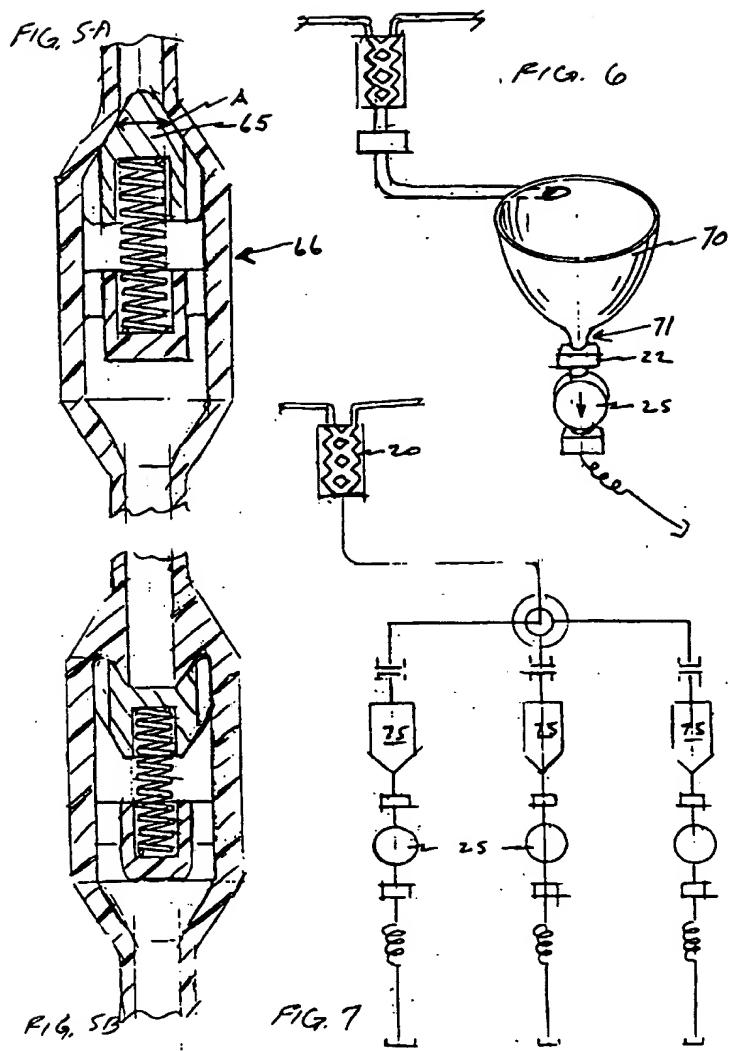


Fig. 1





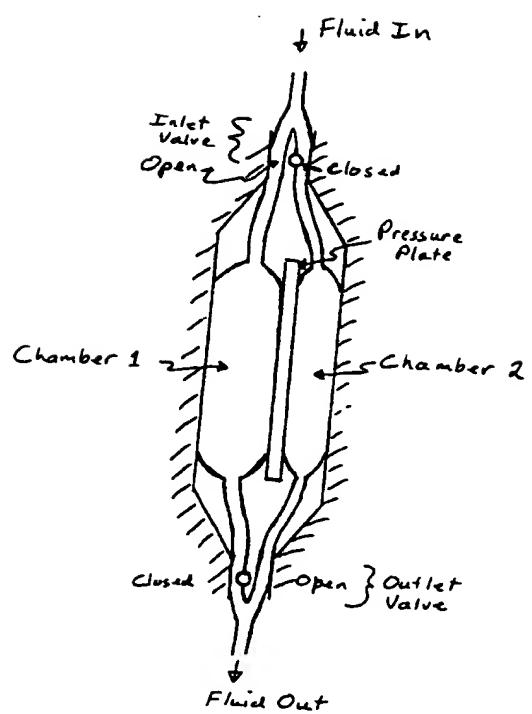


FIG 8

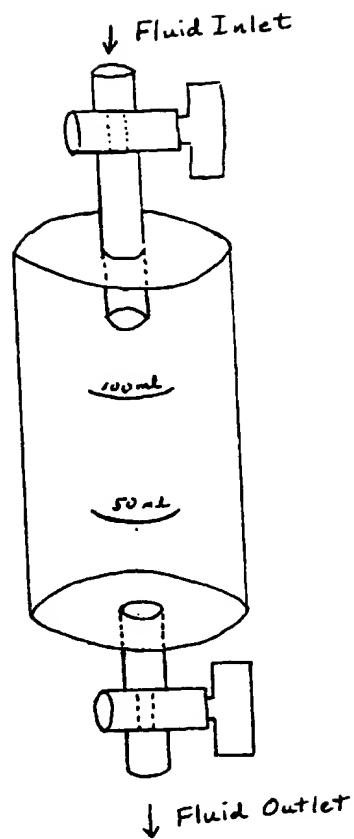


FIG 9

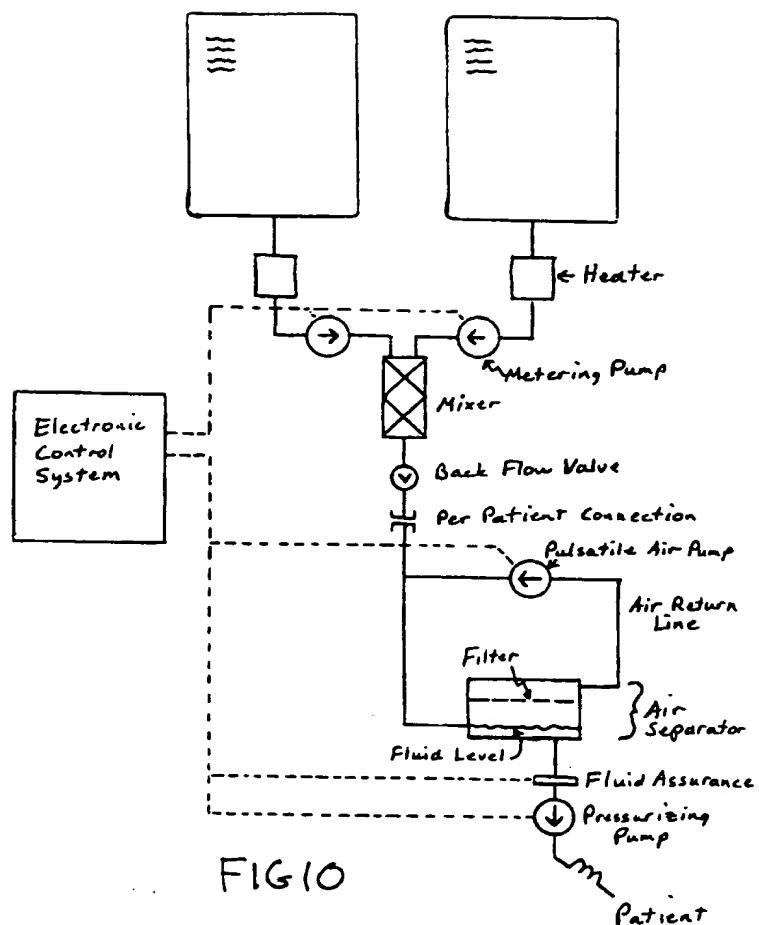


FIG 10



European Patent
Office

EUROPEAN SEARCH REPORT

Application Number
EP 94 11 6908

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int.Cl.)
X	US-A-4 207 871 (JENKINS) * column 1, line 36 - column 2, line 28 * * figure 1 *	1,2	A61M5/14 A61M5/168
A	---	5	
X	US-A-4 798 590 (O'LEARY ET AL.) * column 3, line 67 - column 4, line 27 * * figures 1,2 *	1,4	
X	WO-A-80 01754 (ABBOTT LABORATORIES) * page 6, line 35 - page 9, line 33 * * page 11, line 32 - page 12, line 21 * * figures 2,3 *	5	
X	US-A-4 262 824 (HRYNEWYCT) * column 1, line 67 - column 2, line 55 * * figure 2 *	1,13	
X	US-A-4 038 981 (LEFEVRE ET AL.) * column 5, line 40 - line 58 * * figure 1 *	10	
X	US-A-4 754 786 (ROBERTS) * column 5, line 51 - column 6, line 38 * * figures 4,6 *	12	A61M
A	US-A-4 750 643 (WORTRICH) * column 3, line 14 - column 5, line 5 * * figures 1,3 *	6,8	
The present search report has been drawn up for all claims			
Place of search	Date of completion of the search	Examiner	
THE HAGUE	23 January 1995	Schönleben, J	
CATEGORY OF CITED DOCUMENTS			
X : particularly relevant if taken alone	T : theory or principle underlying the invention		
Y : particularly relevant if combined with another document of the same category	E : earlier patent document, but published on, or after the filing date		
A : technological background	D : document cited in the application		
O : non-written disclosure	L : document cited for other reasons		
P : intermediate document	& : member of the same patent family, corresponding document		